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Initial Performance Evaluation of a Spotted Array Mobile Analysis Platform (MAP) for the Detection of Influenza A/B, RSV and MERS Coronavirus

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Abstract

Clinical samples were evaluated with the Mobile Analysis Platform (MAP) to determine platform performance for detecting respiratory viruses in samples previously characterized using clinical RT-PCR assays. The percent agreement between MAP and clinical results was 97% for influenza A (73/75), 100% (21/21) for influenza B, 100% (6/6) for RSV, and 80% (4/5) for negative specimens. The approximate LOD of the MAP was 30 copies /assay for RSV and 1500 copies/assay for MERS Coronavirus.

Acute respiratory illnesses (ARI) caused by respiratory viruses including influenza viruses and respiratory syncytial virus (RSV) affect hundreds of millions of people per year, and are the most common causes of viral infections in the respiratory tract in humans (Berry, 2015; Zimmerman, 2015; Fendrick, 2003). Each year, approximately 500 million cases of ARI are reported in the United States, with direct and indirect costs approaching $40 billion annually (Berry, 2015; Fendrick 2003).

The 2009 H1N1 pandemic strain of influenza, as well as the H3N2 seasonal variant that circulated during the 2014-2015 season serve as examples of the importance of continued respiratory virus surveillance efforts, and the importance of using accurate and inclusive diagnostics in respiratory virus management (Mahoney, 2010; Mahoney et al., 2011; Flannery, 2016). Additionally, given the emergence of MERS coronavirus and subsequent outbreaks thereof in the Middle East and South Korea, it is important that diagnostic assays for respiratory viruses are rapid and deployable at or near the point of care (POC) (Bhadra, 2015; Raj, 2014). Such diagnostic platforms are becoming more common and are capable of detecting a wide array of respiratory pathogens (Zumla, 2014).

We evaluated a novel, portable, near-POC diagnostic platform, the Mobile Analysis Platform (MAP), by assessing the capability of the MAP to detect influenza A, influenza B and RSV in externally extracted clinical samples, and by establishing the platform's limit of detection (LOD) for RSV and MERS in clinical matrices.

The MAP is a small, portable device integrating disposable assay-specific microfluidic cards (Figure 1). The MAP system is equipped with a set of subsystem to allow automatic assay processing. This includes: (A) a barcode reader to input both specimen and microfluidic card serial numbers; (B) a motorized system to crush liquid reagent packs on command; (C) a

pneumatic system (air pressure and vacuum) to move liquids within the cards via peristaltic pumping using vacuum-actuated midstream valves. Specimens are thus mixed with various reagents pre-packaged into the cards in lyophilized beads to move sample and reagents on the microfluidics card; (D) a set of thermal electric coolers to allow rapid PCR (30 minutes for 40 cycles) PCR cycling of the mixed sample and reagents is performed in a chamber sandwiched between two thermoelectric cooling devices (TECs); (D) Heating elements to maintain temperature at a separate hybridization chamber, (E) an optics system that includes a LED for dye excitation and CCD camera for imaging the microarray; (F) an ARM processor (G) an LCD screen and (H) keypad.

The microfluidics card is disposable and has all the materials required for the assay including (A) sample port to load the swab; (B) wet reagents held in sealed blister packs; (C) lyophilized reagents (D) a microarray chip. The microarray chip consists of 100 μm spots of specific DNA capture probes. The array has 400 of these features, with 100 features reserved for image alignment. This allows up to 300 separate spots for the assay.. PCR products are then digested using uracil deglycosylase and hybridized to a spotted microarray and washed. The microarray is then imaged with a digital camera and LED illumination, and the image is analyzed and statistically interpreted via onboard analysis software. The entire process is fully automated, and results are presented as positive/negative/invalid declarations on the screen of the MAP unit. Multiple primer pair/probe combinations are employed for each analyte, each of which is designed to offer maximum breadth of coverage within the known diversity of the targeted viral genus.

A total of 130 clinical respiratory virus samples were evaluated, including both nasopharyngeal (NP) swab samples resuspended in VTM (N=85) and nasal wash (NW) samples

(N=45) composed of true positives for influenza A (N=93), influenza B (N=21), and RSV (N=7), and samples which were negative for these analytes (N=9). Samples were acquired through institutional review board approved studies (IRB00052743, NHRC.2015.0033) from adults ≥18 years old that were symptomatic for a respiratory virus infection. Influenza A and B samples previously tested positive via the Cepheid Xpert Flu assay (Cepheid, Sunnyvale, CA) or CDC Human Influenza Virus Real-Time PCR Diagnostic Panel (U.S. Centers for Disease Control and Prevention, Atlanta, GA), while RSV samples previously tested positive via a published real-time PCR assay (Templeton, 2004). Limit of detection (LOD) experiments were performed for RSV and MERS by spiking virus into negative clinical matrix. When available, leftover extracts from initial clinical diagnostic testing were utilized. When these were not available, the same methods were used to generate new extracts from waste aliquots of the specimens. Nucleic acids were extracted using either the Arrow Viral NA Kit (NorDiag) or the DSP Viral Mini Kit (Qiagen). Extracted nucleic acid was loaded onto individual MAP assay cards, which were then run and analyzed on portable MAP devices according to manufacturer instructions. Primer sequences for the target organisms can be found in Table 1, with reagent concentrations for the array cards listed in Table 2.

Cycling conditions were as follows: RT step, 5 minutes at 52°C, Hotstart step, 30 seconds at 95°C, extended touchdown PCR and fast PCR, 1 cycle of 7 seconds at 95°C, 1 second at 55°C, 30 seconds at 69.5°C, 2 seconds at 80°C followed by 1 cycle of 7 seconds at 95°C, 1 second at 53.5°C, 30 seconds at 67°C, 2 seconds at 80°C followed by 1 cycle of 7 seconds at 95°C, 1 second at 51°C, 30 seconds at 65°C, 2 seconds at 80°C followed by 1 cycle of 7 seconds at 95°C, 1 second at 50°C, 30 seconds at 63°C, 2 seconds at 80°C followed by 1 cycle of 7 seconds at 95°C, 1 second at 49°C, 30 seconds at 62°C, 2 seconds at 80°C followed by 35 cycles of 7

seconds at 95°C, 1 second at 45°C, 5 seconds at 65°C and 2 seconds at 80°C. All ramp rates on approach to 80°C were dampened to 20% of maximum. Time to result including nucleic acid extraction was 110 minutes per sample. All results are reported here as they appeared on the automated output of the MAP devices. Samples that generated either an invalid result or an error report were recorded as assay failures and were not repeated.

Percent agreement between MAP and standard-of-care RT-PCR results was 97% (73/75) for influenza A-positive samples, with 2 false negative results and 18 assay failures resulting in invalid or error reports. Percent agreement for influenza B was 100% (21/21) with no assay failures, and 100% (6/6) for RSV with one assay failure. Agreement was 80% (4/5) for negative samples, with one RSV positive result and 4 assay failures. The LOD established was 30 and 1500 copies of virus/assay for RSV and MERS Coronavirus respectively.

Previous epidemics and pandemics, as well as the emergence of new respiratory viral pathogens, highlights the need for accurate diagnostic platforms capable of being deployed near the point of care (Zumla, 2014). We performed an evaluation of the MAP prototype to determine its capability to detect and identify influenza A, influenza B and RSV, and performed LOD experiments in clinical matrix for RSV and MERS. Percent agreement between the MAP assay result and the predicate result was high for all pathogens evaluated (97-100%) when excluding invalid assay card results and error reports (no-test instances), and LOD experiments for RSV and MERS yielded acceptable LODs.

An ideal evaluation would have included enough positive and negative samples to calculate sensitivity and specificity at the lower bound of the 95% confidence interval, as opposed to calculating percent agreement. However, based on the limited number of array cards

available for this evaluation, it was more important to evaluate as many positive samples as possible to gauge the capability of the array cards to amplify pathogens.

For MERS, an ideal evaluation would have included clinical samples, however given the rarity and difficulty in acquiring MERS positive clinical samples, this was not possible for this evaluation.

In instances where an invalid result was generated it was almost exclusively the result of variable fluid handling in the array card, which could be overcome by modifying the technology utilized for fluid handling on the MAP unit. Additional improvements to the MAP unit would also include combining the extraction and amplification process into one instrument, which would bring the MAP unit closer to being a POC diagnostic and meeting ASSURED criteria.

Clearly there are limitations to the study, most notably, sensitivity and specificity for the assay were not calculated due to the low number of negative samples evaluated. Future studies would ideally include a large increase in the number of negative samples evaluated, as well as performing the study in a prospective manner.

While this technology is in early stages of development and, as such, yielded a high rate of invalid (no test) results, percent agreement with clinical laboratory methods approached 97% for completed tests. This technology shows promise as a rapid, accurate, deployable diagnostic technology for automated detection and discrimination of multiple pathogens in clinical sample extracts.

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Table 1. Primer Sequences and Targets for MAP Respiratory Virus Array

Organism	Molecular Target	Product size (bp[a])	Primer Name	Sequence
Influenza A	M1	110	VIR13095F	TCAGGCUCCCUCAAAGCCGA
			VIR13096R	/5MAXN[b]/TGCAGGATTGGTCTTGTCTTTAICCA
Influenza A	PA	74	VIR13099F	CTUGAGAAUTUAGAGCCUATGUIGAUGG
			VIR13100R	/5MAXN/CACATTTGAGAAAGCTTGCCCTCAAT
Influenza B	PB1	83	VIR13470F	CAGGCAGCAAUTUCAACAACATUCCC
			VIR13471R	/5MAXN/TTGTCTATTGTGTAGCCTGTTCCTGTTC
Influenza B	PA	78	VIR13491F	GGAGGGAAAAAUCUGTGUACCTGUATUGC
			VIR13492R	/5MAXN/TAGCTTCCATTCCCCATTTCATTTGGAT
RSV	Matrix Protein	83	VIR13361F	AAGAUGGGGCAAAUAUGGAAACAUACGUGAA
			VIR13363R	/5MAXN/TAGAACATTGTACTGAACAGCTGCTGTGTA
			VIR13362R	/5MAXN/TAGGACATTGTATTGAACAGCAGCTGTGTA
RSV	Phosphoprotein	84	VIR13355F	TCGGCUCGUGAUGGAAUAAGAGAUGC
			VIR13357F	TCUGCUCGGGAUGGUATAAGAGAUGC
			VIR13356R	/5MAXN/CGTCATTAATGCTTCAGTTCTGATTTTTTCTATCAT
			VIR13358R	/5MAXN/CGTCATTAATGCTTCTGCTCTTATTTTTTCTATCAT
MERS	Orf1A Protein	92	VIR13088F	CGGCCUUCAACUGGUUGUUGUU
			VIR13089R	/5MAXN/AGCATAATTGTATGACCGCCAGTC
MERS	N Protein	102	VIR13090F	CCUGUGUACUUCCUUCGGUACAGU
			VIR13091R	/5MAXN/GTAGGCATCAATATTTTGCTCAAGAAGC

Table 1. Organism targets, predicted PCR product size, primer name and primer sequences are listed here. a-base pairs b-5MAX (NHS ester)

Table 2. Reagent Concentrations for the MAP Respiratory Virus Assay Cards

UDG (Excipient X4) - 100ul in digestion well
10 Units UDG
3% Trehalose
1.5 mM Tris
7.5 mM KCL
0.015 mM EDTA
0.15 mM DTT
0.0015 % BSA
50.00 nM Hybridization Control
Kapa (Excipient X2.2) - 150ul in PCR Master Mix chamber
16 Units Kapa
2 % Trehalose
266.67 uM dNTP mixture
4.67 mM $MgCL_2$
1.33 X Buffer A
SSIII (Excipient A) - 150ul in MM chamber[c]
50 Units SuperScript III
2 % Trehalose
5 mM Tris
1 mM Ammonium Sulfate
1.2 mM $MgCL_2$
0.005 % Tween-40
0.4 mM DTT
0.015 µg random primers
0.03 µg Poly-A

Table 2. Composition of each of the three lyophilized bead reagents provided with the Map

cards, and the resulting reagent concentrations or compositions following resuspension thereof in

the chambers of the card in which the beads were packages is represented. Super Script III (Life

Technologies, Carlsbad, CA)

Figure 1